

# Lower extremity muscle strength reference values for young Saudi male adults aged 21 to 23 years and their correlation with anthropometric parameters and balance

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## Abstract

Normative reference values for muscle strength are needed for muscle strength assessment and estimation of prognosis in lower extremity related neuromuscular disorders, as muscle strength influenced by anthropometric parameters and muscle strength itself affects balance. Normative reference values for muscle strength in the Saudi Arabian population is lacking in the literature. Hence, the current study aimed to establish normative reference values for lower extremity muscle strength and to correlate these values with anthropometric parameters and balance. Lower extremity muscle strength and balance were assessed by baseline hand-held dynamometer and by forward, lateral, and oblique direction reach tests in 421 young male adults between 21 and 23 years of age. The mean and standard deviation of lower extremity strength ranged from  $43.83 \pm 16.92$  lb to  $62.07 \pm 10.74$  lb. Body weight, body mass index, and oblique and lateral reach distances were correlated with some knee and ankle muscle strength values. Body weight, body mass index, and balance showed significant effect on lower extremity muscle strength. Furthermore, decreased muscle strength may impair balance; the current clinical practice should evaluate body weight, body mass index, and muscle strength during the assessment process.

**Key words:** lower extremity muscles, reference values, correlations, balance

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## Introduction

Muscle strength is defined as a muscle's ability to generate force ([Higgins 2011](#)). Muscle strength is critically important for functional performance ([Powers et al. 2006](#); [Higgins 2011](#)). Young adults demonstrate high levels of muscle performance compared with their elders; as age increases, muscle performance decreases ([Stoll et al. 2000](#)). Adequate muscle strength at a young age is important for aesthetics and is crucial for sports performance and injury prevention ([Bourne et al. 2018](#); [Soylu et al. 2019](#)). Many disorders in young adults, including obesity, malnutrition, issues with mental health, technology or internet addiction, drugs, alcohol, and smoking, can be mitigated by participating in physical activities like muscle strengthening ([World Health Organization 2014](#); [Lam and Riba 2016](#);

Foster et al. 2018; Cangin et al. 2018). The management of these disorders requires normative reference values for muscle strength to accurately understand muscle capacity (Bhattacharyya et al. 2017).

Many studies have identified reference values for muscle strength (Bisen et al. 2012; Leong et al. 2016; McKay et al. 2017). However, normative reference values for young adults are not well established, as this population is rarely studied except as a part of larger age groups (Bohannon 2011). Because muscle strength declines in old age, chronic diseases that affect muscle strength are most common in the elderly (Francis et al. 2017); therefore, research has focused more on establishing reference values in the elderly rather than in young healthy populations. Muscle testing methods have changed over time; just a few decades ago, manual muscle testing was a common clinical method for assessing muscle strength (Fisher and Harrington 2015). Even though it is an ideal method in clinical practice, it does not have good reliability and validity for the assessment of muscle strength (Cuthbert and Goodheart 2007). The most common objective methods for assessing muscle strength are isokinetic and portable dynamometers (Benfica et al. 2018). Other tools that assess muscle strength, such as the leg press, plate spring gauge, and pull down, show good reliability, but validity has not been proven for these tools (Mijnarends et al. 2013; Alqahtani et al. 2017). The isokinetic dynamometer is considered the ideal muscle testing method, and it provides both isokinetic (concentric and eccentric) and isometric measures (Benfica et al. 2018); however, the hand-held dynamometer and myometer are currently very popular in clinical use because of their availability and low cost, and they provide isometric measures. The hand-held dynamometer has been shown to have good reliability and validity in clinical use. (Mentiplay et al. 2015).

Many factors can affect muscle strength, including age, gender, anthropometric parameters, nutritional status, and physical activity. Muscle strength has been positively correlated with function, balance, and gait in many disease populations. (Kamat et al. 2012; Wang et al. 2016; Callesen et al. 2019). Anterior cruciate ligament, meniscal injuries due to road traffic accidents, and ankle sprains are common in young healthy population, leading to reduced lower extremity muscle strength as the primary impairment (Thomas et al. 2013). In clinical practice, rehabilitation of these individuals requires reference values for muscle strength in the young, healthy population.

However, the factors that affect muscle strength in young populations are not extensively established due to a lack of literature. In the Kingdom of Saudi Arabia, reference values for muscle strength have been commonly confined to the hand (Alahmari et al. 2019), and normative reference values taken with a hand-held dynamometer for the remaining muscles are scarce. There is a high incidence of road traffic accidents in the Kingdom of Saudi Arabia, and many of the victims, most of whom are young males, experience head, neck, and upper and lower extremity injuries (Mansuri et al. 2015). In addition, the obesity rate in the Kingdom of Saudi Arabia is 33.7%, making it the 15th most obese country in the world (Alqarni 2016; Habbab and Bhutta 2020). Moreover, many Saudi Arabian children are addicted to smartphones, games, and the internet, which further exacerbates obesity in the young adult population (Albursan et al. 2019). Both accidents and obesity have an effect on muscle strength.

Improving muscle strength is a critical intervention that is required to address these issues; hence, normative data is needed to prescribe strengthening program parameters and to estimate progress. The current study aims to establish normative reference values for lower extremity muscle strength in the young adult population of Saudi Arabia using a hand-held dynamometer and to assess the correlation between strength and anthropometric parameters and balance.

## Methodology

Approval for this cross-sectional study was obtained from the institutional ethical review board (approval no. REC # 2016-08-29). The sample size calculation was performed online using Calculator.net software. A total sample size of 424 was determined based on a 95% confidence interval, 5% margin of error, population proportion of 50% of the expected sample size, and 10% dropout rate.

Using computer-generated numbers, we recruited college students randomly for a duration of six months. The study was conducted in the Department of Medical Rehabilitation Sciences, College of Applied Medical Sciences, King Khalid University, Abha, Saudi Arabia, and we chose college-going students aged 21–23 years because that is a vulnerable age for accidents, addictions, and obesity. A total of 424 male students with no history of lower extremity fractures or ligament injuries were included in the study. Students with any congenital, neurological, or debilitating diseases were excluded from the study. Students who were suffering from a cold, fever, or infection; who were taking any medication that alters muscle contraction; or who were suffering from any acute pain such as back pain, neck pain, delayed onset muscle soreness, or muscular aches were also excluded. The included students were introduced to the research aims and asked to complete a written informed consent.

Demographic characteristics, including age, height, weight, upper limb length, trunk length, and lower limb length, were measured and entered in the data entry sheet. To measure upper limb length, we measured from the acromion process of the shoulders to the radial styloid process; for measuring lower limb length, we measured from anterior superior iliac spine on the pelvis to the medial malleolus; for measuring trunk length, we measured from the acromion process of the shoulder to the anterior superior iliac spine on the pelvis. All the length measurements were taken using a tape measure in centimeters. The validity of the measurements was proved by comparing them with a computed tomographic scan for measuring limb length (Neelly et al. 2013). The lower extremity muscle groups included in this study were hip flexors, extensors, abductors, adductors; knee flexors and extensors; and ankle plantar flexors and dorsiflexors. A baseline hydraulic push–pull dynamometer of 250 lb with an analog (dial) gauge (Model: FEI-12-0394, Fabrication Enterprises Inc., USA) was used for muscle strength assessment. This instrument has good concurrent validity by comparison with isokinetic dynamometers for testing hip, knee, and ankle muscles (Mijnarends et al. 2013). We used the “make test” for the assessment process, in which the participant exerted force against the dynamometer for 3–5 s. We followed the standard method of dynamometer assessment, and the protocol for the starting position, therapist position, and placement of the dynamometer was based on Tedla et al. (2012). The students were provided detailed instructions for the muscle strength assessment, and we obtained muscle strength values three times for each muscle group (Kelln et al. 2008) as shown in Fig. 1. The average of the three measurements was used for the analysis. If there was a difference of more than 10 lb between each measurement, we performed additional trials to ensure that there were no mistakes in the values obtained. Between each muscle group measurement, at least 30 s of rest was provided to decrease fatigue. Balance was assessed using the standard procedures for the forward, lateral, and oblique direction reach test. A piece of graph paper was affixed to a movable white board. The subject was asked to stand in a relaxed position with legs shoulder width apart and without shoes, and the white board was placed parallel to the forward center line to them. To measure the forward reach, the participants were instructed to raise their arm to shoulder level and to keep their arms parallel to the graph paper on the white board. The starting position was recorded with a pen mark on the graph paper with the tip of third metacarpal as reference point. Participants reached forward as far as possible without raising their heels or taking a step. The end position was also recorded on the graph paper with a pen mark. The difference between the end position and the starting position was measured in centimeters. The lateral reach and oblique direction reach were also



**Fig. 1.** Muscle strength testing of lower extremity muscles by hand-held dynamometer. Muscle strength testing of: (a) hip flexors, (b) hip extensors, (c) hip abductors, (d) hip adductors, (e) knee extensors, (f) knee flexors, (g) ankle dorsiflexors, and (h) ankle plantar flexors.

measured in a similar manner by changing the position of the participants and the white board, as explained by [Tedla et al. \(2021\)](#).

Data collection took 30–45 min per subject in one or two sessions, depending up on the subject's fatigue level. If the subject's assessment was planned in two sessions, then the duration of the two sessions was not more than one hour in total.

## Statistical analysis

We used IBM SPSS Statistics for Windows Version 22.0 (Armonk, NY: IBM Corp.) for the data analysis. Descriptive statistics were performed to calculate the mean, standard deviation, minimum, and maximum. An assessment of the normality of the data was conducted using the Shapiro–Wilk test. Differences between the right and left sides were calculated using an independent *t*-test, and correlations between variables were measured using the Pearson correlation coefficient. Based on the guidelines provided by [Schober and Schwarte \(2018\)](#), we interpreted the *r* value as follows: 0.00–0.10, negligible correlation; 0.10–0.39, weak correlation; 0.40–0.69, moderate correlation; 0.70–0.89, strong correlation; and 0.90–1.00, very strong correlation.

**Table 1.** Mean, standard deviation, minimum and maximum of demographic characteristics, and balance test variables.

Variables	Mean $\pm$ standard deviation	Minimum	Maximum
Age (years)	21.93 $\pm$ 0.74	21	23
Height (m)	1.69 $\pm$ 0.04	1.6	1.77
Weight (kg)	73.99 $\pm$ 17.67	50	118
Body mass index (wt/m <sup>2</sup> )	26.04 $\pm$ 6.32	17.72	45.52
Upper limb length (cm)	57.03 $\pm$ 2.91	52	64
Trunk length (cm)	49.30 $\pm$ 2.90	44	57
Forward reach (cm)	31.39 $\pm$ 4.62	22.5	41
Lateral reach (cm)	23.78 $\pm$ 4.61	13.33	33
Oblique direction reach (cm)	25.48 $\pm$ 4.98	18	42.67

## Results

The descriptive statistics for demographic characteristics, including age, height, weight, body mass index (BMI), upper limb length, lower limb length, and trunk length, as well as the balance measurements are provided in [Table 1](#). The normative reference values for lower extremity muscle strength, presented as means and standard deviations, minimums and maximums, and *p* values for right- and left-side differences, are provided in [Table 2](#). In the analysis of side-to-side differences, only the hip flexors and knee extensors had statistically significant differences between the right and left sides, with *p* values of 0.003 and 0.014, respectively. The correlations between muscle strength and upper extremity length, trunk length, lower extremity length, height, weight, BMI, age, and balance were calculated. Of all the variables, weight, BMI, forward reach distance, and oblique reach distance had positive correlations with strength. Weight had a moderate correlation with left hip flexors and right and left knee extensors, with correlation *r* values (*p* values) of 0.40 (0.03), 0.526 (< 0.001), and 0.579 (< 0.001), respectively. In contrast, weight had a weak correlation with left hip abductors, with a correlation *r* value (*p* value) of 0.362 (0.05). Similarly, BMI had a moderate correlation with left hip flexors, abductors, and right and left knee extensors, with correlation *r* values (*p* values) of 0.440 (0.02), 0.415 (0.02), 0.536 (< 0.001), and 0.602 (< 0.001), respectively. The details are provided in [Table 3](#).

Balance as tested by forward reach, lateral reach, and oblique reach distances showed some interesting findings. No muscle strength values were correlated with forward reach distance, whereas lateral reach and oblique reach demonstrated some moderate correlations with strength. Lateral reach had a moderate correlation with right and left knee extensors and right ankle dorsiflexors, with correlation *r* values (*p* values) of 0.451 (0.01), 0.512 (< 0.001), and 0.504 (< 0.001), respectively. Lateral reach had a weak correlation with left ankle dorsiflexors, with a correlation *r* value (*p* value) of 0.379 (0.04). Oblique reach had a moderate correlation with right and left knee extensors and right ankle dorsiflexors, with correlation *r* values (*p* values) of 0.451 (0.01), 0.512 (< 0.001), and 0.504 (< 0.001), respectively.

## Discussion

These are the first normative reference values to be established for lower extremity muscle strength in young adults in Saudi Arabia, and the correlation analysis between various demographic



**Table 2.** Mean, standard deviation, minimum and maximum of muscle strength values, and p values of the side differences.

Muscle group and side	Mean $\pm$ standard deviation	Minimum	Maximum	<i>p</i>
Right hip flexors	62.07 $\pm$ 10.74	37.67	90	0.003**
Left hip flexors	59.04 $\pm$ 9.58	38.67	83.33	
Right hip extensors	57.24 $\pm$ 10.97	36.67	80.33	0.467
Left hip extensors	56.39 $\pm$ 12.72	27.33	87.33	
Right hip abductors	66.62 $\pm$ 12.78	40.33	95.67	0.227
Left hip abductors	64.46 $\pm$ 12.43	34	106.67	
Right hip adductors	43.83 $\pm$ 16.92	18.67	89	0.165
Left hip adductors	46.09 $\pm$ 18.32	19	83.33	
Right knee extensors	55.81 $\pm$ 10.35	32.33	78.33	0.014*
Left knee extensors	53.88 $\pm$ 10.24	36.67	79.33	
Right knee flexors	58.13 $\pm$ 9.12	41.67	76	0.166
Left knee flexors	56.44 $\pm$ 9.69	35	76	
Right ankle dorsi flexors	50.77 $\pm$ 7.85	33.33	71.67	0.315
Left ankle dorsi flexors	49.89 $\pm$ 7.34	41	77	
Right ankle plantar flexors	45.69 $\pm$ 12.46	24.67	75	0.394
Left ankle plantar flexors	44.67 $\pm$ 15.04	24.33	83.33	

**Note:** \*Correlation is significant at the 0.05 level (2-tailed). \*\*Correlation is significant at the 0.01 level (2-tailed).

characteristics and balance and muscle strength revealed interesting findings. Previous researchers who proposed normative reference values for lower extremity muscle strength for the populations of Switzerland (Stoll et al. 2000), Brazil (Daloia et al. 2018), and Australia (Stoll et al. 2000) reported normative values similar to those found in our study for many of the muscle groups. In our study, we found a moderate correlation between BMI and left hip flexors, abductors, and right and left knee extensors, with correlation *r* values (*p* values) of 0.44 (0.02), 0.415 (0.02), 0.536 (0.001), and 0.62 (0.001), respectively. Pasco et al. (2020) conducted a study in the Southeastern Australian population between the ages of 20 and 97 years and established a weak and positive correlation between BMI and muscle strength: for males, *r* = 0.16 for hip flexors (*p* = 0.058), and *r* = 0.13 for hip abductors (*p* = 0.002). In contrast to our study, the correlation between the BMI and muscle strength was weak in their study. This could be because the ages of the included participants covered a wider age range, from 20 to 97 years, and also because the total number of young males included in their study was comparatively less than the middle and older age groups.

Stoll et al. (2000) found significant differences in the right- and left-side muscle strength of the hip adductors, hip external rotators, hip flexors, knee flexors, ankle dorsiflexors, and ankle plantar flexors. Our study found significant differences between right and left hip flexors and knee extensors. Except for hip flexors, the muscle groups found in the study by Stoll et al. (2000) differ from those found in our study, and we believe that the differences can be attributed to differences in the type of muscle strength measurement performed. They measured muscle strength in kilopascals, and we measured strength in pounds. Compared with pounds, kilopascals are quite minute, which could explain the larger differences between the right and left sides seen in the previous study. These measurement unit

**Table 3.** Showing correlation  $r$  and  $p$  values between demographic characteristics, balance, and muscle strength.

Variables Correlated		$r$	$p$
Weight (kg)	LHF	0.398*	0.03
	RKE	0.526**	0.00
	LKE	0.579**	0.00
	LHAB	0.362*	0.05
Body mass index (wt/m <sup>2</sup> )	LHF	0.440*	0.02
	RKE	0.536**	0.00
	LKE	0.602**	0.00
	LHAB	0.415*	0.02
Lateral reach (cm)	RKE	0.451*	0.01
	LKE	0.512**	0.00
	RADF	0.504**	0.00
	LADF	0.379*	0.04
Oblique direction reach (cm)	RKE	0.412*	0.02
	LKE	0.377*	0.04
	RADF	0.457*	0.01
	LADF	0.462*	0.01
	RAPF	0.403*	0.03

**Note:** \*Correlation is significant at the 0.05 level (2-tailed). \*\*Correlation is significant at the 0.01 level (2-tailed).  $R$ , Pearson correlation coefficient value;  $p$ , probability value; BMI, body mass index; LHF, left hip flexors; RKE, right knee extensors; LKE, left knee extensors; LHAB, left hip abductors; RADF, right ankle dorsi flexors; LADF, left ankle dorsi flexors; RAPF, right ankle plantar flexors.

variations among studies may be the reason for the differences in the results. In addition, differences in the age groups and muscle testing methods could significantly influence the muscle strength values obtained. The muscle strength of right hip flexors and knee extensors was high compared with left-side hip flexors and knee extensors. This could be due to the usage of the right side in many activities of daily living. The repeated use of a dominant side creates efficient neural connections from the brain and leads to greater strength (Daloia et al. 2018).

Another finding of note in our study was the correlation between body weight and BMI and some muscle groups, including hip flexors and knee extensors. Similar results were obtained by Nobuyuki et al. (2012) who studied the influence of anthropometric parameters on muscle strength in Japanese adolescents. Nobuyuki et al. (2012) also found high correlations between height and leg muscle strength, which we did not find in our study.

The correlations between the reach tests and muscle strength found in our study were similar to those of previous studies. Oya et al. (2008) confirmed the importance of knee extensor muscle strength assessment in the identification of fall risk in the elderly and reported that insufficient knee extensor muscle activity can increase fall risk. Our study found a similar relation between knee extensor muscle

strength and lateral and oblique reach distances. While some authors have discussed that ankle dorsiflexor and hip abductor muscle activity can influence balance, there has not been concrete evidence of this (Newton 2001). This is because the direction of movement of the center of gravity on the base of support can initiate complex muscle combinations depending on need (Kazemi et al. 2017). In the general population, any reach beyond the base of support causes an initiation of distal ankle strategy muscles. As the reach distance increases, the activity is shifted to more proximal muscles and finally leads to a step if the muscles fail to control the center of gravity. It is difficult to determine which muscle synergy will be active in each reach direction, and muscle activity changes as the direction of the reach changes (Afschrift et al. 2016). Because of the center of gravity shift during oblique direction and lateral direction tests, we assume that the ankle dorsiflexors and knee extensors played an important role in controlling the center of gravity, which explains the positive correlation between the muscle strength of these muscle groups and the reach test distance.

The data collection process was tedious and time consuming. We managed the data collection by planning the examination in various stations. The subjects were moved from one station to another station with sufficient rest. As the subject population was young males, we did not encounter any difficulty during the data collection; a few people experienced fatigue, but they recovered within a few minutes and continued the remaining examination without any discomfort.

Due to cultural issues and practical difficulties, we considered only male subjects from a single university, and the age group included was young adults between 21 and 23 years of age because that was the only age group available at our university campus. In the future, we suggest involving both genders and various age groups from multiple centers and the use of more advanced outcome measures such as isokinetic dynamometers and pressure platforms. The effect of physical activity and fatigue also should be considered in future studies. This may provide more culturally robust and sensitive data related to muscle strength in the population of the Kingdom of Saudi Arabia.

## Conclusion

This research established reference values for lower extremity muscle strength in young male adults in Saudi Arabia. Mean and standard deviation of muscle strength ranged from  $43.83 \pm 16.92$  lb to  $62.07 \pm 10.74$  lb. Body weight, BMI, lateral reach distance, and oblique reach distance had positive correlations with lower extremity muscle strength values.

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## Author contributions

JST, DRS, and RSR conceived and designed the study. JST, KG, and VNK performed the experiments/collected the data. JST, DRS, KG, and PSS analyzed and interpreted the data. JST, RSR, VNK, and PSS contributed resources. JST, DRS, RSR, KG, VNK, and PSS drafted or revised the manuscript.

## Conflicts of interest

The authors certify that no conflict of interest exists.

## Data availability statement

All relevant data are within the paper.



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